Practical Phantom Studies with A Battery Based Electrical Impedance Tomography System

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Abstract—Electrical impedance tomography (EIT) is a computed tomographic technique which has been applied for a number of medical investigations. Practical EIT systems need an electronic instrumentation system for current injection and voltage data collection from the patient's body. EIT instrumentation is generally fed by the ac main power supply which must be developed with a number of strictly specified design parameters and must be applied with certain cares for obtaining the better patient safety. To obtain a better patient safety a battery based EIT system developed and studied with practical phantoms. A battery based EIT system is developed with a LabVIEW based EIT instrumentation powered by a battery based power supply. A number of practical phantoms are developed and the resistivity images are studied with battery based EIT system. Signal to noise ratio is improved in battery based EIT system. Results demonstrated that the practical phantoms are successfully reconstructed with battery based EIT system. Results also show that all the phantom domains with different inhomogeneity configurations are successfully reconstructed from the boundary data measured.

Keywords—Electrical impedance tomography (EIT), battery based EIT, medical imaging, patient safety, practical phantoms, image reconstruction, resitivity imaging.

I. INTRODUCTION

Electrical impedance tomography (EIT) [1-8] is a computed tomographic technique [9-10] which reconstruct the spatial distribution of electrical impedance data of a domain under test from the boundary voltage current data using a reconstruction algorithm [11-15]. Being a fast, noninvasive, radiation free, portable low cost imaging modality, EIT is a computed tomographic imaging modality which has been applied for a number of medical and clinical investigations [16-17]. In medical and clinical studies patient safety [1, 18] is very crucial factor which must be considered before applying a diagnostic technique on patients. Biomedical electronic instruments and health monitoring systems [19-20] powered by ac mains are generally provided with some precautions and patient safety guidelines for it safer application in medical investigations. Practical EIT systems (Figure 1) are developed with an EIT electronic instrumentation system [21-26] required for current injection and voltage data collection from the patient's body through surface electrodes [27-30]. The electronic instrumentation of the

EIT system is generally fed by the ac main power supply using a step down transformer and the rectifier-filter circuits. Therefore the EIT instrumentation fed by ac mains must be designed and developed with a number of design parameters which must be followed by the designers should be strictly specified in the instrument data sheet along with the required precautions. Moreover the ac mains powered EIT system must be applied to the patients by taking certain precautions to obtain the better patient safety. Also, medical EIT systems must be studied, tested, evaluated and calibrated with practical phantoms [3, 6, 14-15, 31-40] before applying it to human subjects. In this direction, to provide a better patient safety, a battery based EIT system is developed and studied with practical phantoms. A battery based EIT system is developed with an EIT instrumentation powered by a battery based regulated power supply (BRPS) as shown in Figure 2. A number of practical phantoms are developed with different inhomogeneity configurations and the resistivity images are studied with battery based EIT system. Results demonstrated that the signal to noise ratio (SNR) [41-42] of the boundary potential data is improved in battery based EIT system. It is observed that the practical phantoms with different inhomogeneity configurations are successfully reconstructed from the boundary data measured collected battery based EIT system.



Fig. 1. EIT system schematic with a patient with surface electrodes.

II. MATERIALS AND METHODS

A. Battery Based EIT System

Battery based EIT system is developed with an electronic instrumentation powered by a battery based regulated power supply (BRPS). The EIT instrumentation is interfaced with the personal computer (PC) with a graphical user interface working on LabVIEW [43-45]. LabVIEW based EIT instrumentation is developed with a constant current injector (CCI) [46], an automatic electrode switching module (ESM) and a LabVIEW based data acquisition system (DAS). A battery based regulated power supply (BRPS) is developed with two 12 V sealed lead acid rechargeable batteries and a battery charging circuit module (BCCM) developed for generating a pure ± 12 V pure dc power. The BCCM is used for charging the batteries of the BRPS and the BRPS is used to feed the entire EIT instrumentation.



Fig. 2. Schematic of the battery based regulated power supply (BRPS) with filter-regulator-filter (FRF) block.

The BCCM is developed with a filter-regulator-filter (FRF) block developed as per the battery power consumption. The BCCM is fed by the power supply obtained from the bridge rectifier circuit module (BRCM). The battery charging circuit is used for charging the batteries of the BRPS and the charging circuit is kept disconnected when the BRPS is used for feeding the EIT system. The entire analog instrumentation of the developed EIT system (Figure 3) is fed by the BRPS and the EIT current injection and the boundary data collection are performed with a number of practical phantoms.



Fig. 3. The complete battery based EIT system.

B. Practical Phantoms

Practical phantoms are developed with glass tanks filled with NaCl solution as the low resistive background medium and the vegetable cylinders as the high resistive inhomogeneities. Shallow glass tanks are used as the phantom tank and the tanks are filled with NaCl solution. Sixteen stainless steel electrodes are cut from a 100 μ m thick high quality stainless steel sheet (Type 304) and the electrodes are fixed with steel paper clips. All the electrodes are connected with low resistive flexible copper wires using alligator clips and the electrode connection are made with the EIT instrumentation. A number of vegetable cylinders are kept at different electrode positions and a number of phantoms are made for EIT studies. Figure 4 shows a NaCl-carrot phantom with NaCl solution as the background medium and a carrot cylinder near electrode number 3 (E3) as inhomogeneity. The electrical resistivity of the carrot tissues are also measured by the QuadTech 7600 (QuadTech Inc., USA) to compare the reconstructed resistivities with the actual resistivity.



Fig. 4. NaCl-carrot phantom with carrot cylinder near electrode 3 (E3) as the inhomogeneity.

C. Boundary Data Collection

The boundary voltage data are collected from a number of practical phantoms using the battery based EIT system. The Figure 1 shows the 16-electrode battery based EIT system with a patients with surface electrodes attached to its body surface at the plane (cross section of the body) under diagnosis. As shown in the figure, the system generates a constant voltage signal with different frequency points using a multifrequency signal generator and the voltage signal is converted to a constant current signal by a voltage controlled current source (VCCS). The constant current signal is injected to the patient's body at different frequencies through the current electrodes or driving electrodes and the surface potentials are measured at the voltage electrodes or sensing electrodes using the LabVIEW based data acquisition system (DAS). Surface electrodes are switched in a particular switching fashion called current injection pattern or current injection protocol which allows us to conduct the current injection and voltage measurement through using an automatic electrode switching module (A-ESM) developed with analog multiplexers (MUX). 1 mA, 50 kHz constant sinusoidal current is injected to the phantom boundary and the potential data are collected from all the electrode with opposite current injection protocol. In opposite current pattern the current signal is injected through two opposite electrodes (180° apart in space) and the potential data are measured on the other electrodes. In the present study the potential data developed on the domain boundary are collected from all the electrodes. In the sixteen electrode phantoms developed in the present studies, a complete scan provided 256 boundary data though it is observed that only 128 data collected from the first eight current projections are sufficient for image reconstruction. Boundary data are collected are collected from all the

phantoms and the data are used for image reconstruction using the image reconstruction algorithm in PC.

D. Resistivity Imaging of Phantoms

The resistivity images are reconstructed from the boundary data collected from all the practical phantoms using Electrical Impedance Tomography and Diffuse Optical Tomography Reconstruction Software (EIDORS) [47-49]. The EIDORS is a Matlab based EIT or DOT (Diffuse Optical Tomography) image reconstruction software which works on the Gauss-Newton approach. In the present study the EIDORS is modified as per the phantom configuration and the forward and inverse problems both are solved with a FEM mesh containing 1968 elements and 1049 nodes. All the image reconstruction processes are conducted with Levenberg-Marquardt Regularization method (LMR) method implemented in EIDORS.

III. RESULTS AND DISCUSSION

The Fig. 5 shows the resistivity image reconstructed from the NaCl-carrot phantom shown in the Figure 4 at 12.5 kHz. Experimental results obtained from the electrical impedance spectroscopy conducted by QuadTech 7600 show that the carrot tissue has a resistivity around 160 Ω m. It is observed that the carrot inhomogeneities as well as the NaCl background are properly reconstructed in the resistivity image as the carrot regions are found with higher resistivity values in the reconstructed images. Results show that the resistivity profile of the background and the inhomogeneity matches with the original resistivity profiles of the NaCl and carrot respectively though the carrot resistivity is under estimated.



Fig. 5. Resistivity image of the NaCl-carrot phantom (shown in Figure 4) with carrot cylinder near electrode 3 (E3) as the inhomogeneity.

Fig. 5 shows that the reconstructed carrot resistivity is around 7 Ω m at 12.5 kHz which is low compared to the original carrot resistivity. The reason behind the underestimation of carrot cylinder is the large difference between the NaCl conductivity and carrot conductivity. The EIT technology is suitable for the domain containing the materials with low resistivity differences such as the tumor and the normal tissue. But for laboratory studies saline and high resistive materials such as nylon cylinders [3, 8] polypropylene cylinders [6], etc. In the present study the vegetables are used as the high resistive materials to test a battery based multifrequency EIT system as the impedance of the vegetables vary with frequency but nylon or other plastic materials fails to show the frequency depended impedance. The present research study is conducted with different frequencies but due to the results on 12.5 kHz has been presented as per the scope of the paper. The reconstructed resistivity of the carrot tissues is found decreasing with frequencies in multifrequency impedance imaging with the developed battery based EIT system and which correlates with the measured resistivity values obtained by the impedance analyzer. In all the frequencies the carrot tissue are reconstructed with more than the reconstructed NaCl resistivity but decreasing with frequencies. The impedance of the biological tissue decreases with frequencies as the cell membrane of biological cells allow more current to pass through it at higher frequencies [35].

IV. CONCLUSIONS

A battery based electrical impedance tomography (EIT) system is developed a battery based regulated power supply (BRPS) for better patient safety in medical imaging. The EIT instrumentation is developed with a constant current injector (CCI), an automatic electrode switching module (ESM) and a LabVIEW based data acquisition system (DAS) and all the instrumentation blocks are fed by BRPS. The battery based EIT instrumentation is studied for constant current inject and boundary data collection in EIT. A number of practical phantoms are developed and the resistivity imaging studies are conducted with battery based EIT system developed. Results show that the vegetable inhomogeneities as well as the NaCl backgrounds are properly reconstructed in the resistivity images. Results also show that the resistivity profiles of the reconstructed phantom domains match with their original resistivity profiles but the vegetable resistivity is under estimated due to the large difference between the vegetable and NaCl resistivity.

References

- [1] J. G. Webster, Electrical Impedance Tomography. Bristol and New York: Adam Hilger; 1990.
- [2] T. K. Bera and J. Nagaraju, Electrical Impedance Tomography (EIT): A Harmless Medical Imaging Modality, Research Developments in Computer Vision and Image Processing: Methodologies and Applications, Ch. 13, pp 224-262, IGI Global USA.
- [3] T. K. Bera and J. Nagaraju, Studies on The Thin Film Based Flexible Gold Electrode Arrays for Resistivity Imaging in Electrical Impedance Tomography, Measurement 47 (2014) 264-286.
- [4] D. S. Holder, Electrical Impedance Tomography: Methods, History and Applications. Bristol and Philadelphia: IOP Publishing; 2005.
- [5] T. K. Bera and J. Nagaraju, A MATLAB Based Boundary Data Simulator for Studying The Resistivity Reconstruction Using Neighbouring Current Pattern, Journal of Medical Engineering, Volume 2013, Article ID 193578, 15 pages.
- [6] T. K. Bera and J. Nagaraju, Resistivity Imaging of A Reconfigurable Phantom With Circular Inhomogeneities in 2D-Electrical Impedance Tomography, Measurement 44 (2011) 518-526.
- [7] J. K. Seo, E. J. Woo, Nonlinear Inverse Problems in Imaging, Wiley; 1 edition (December 26, 2012)
- [8] T. K. Bera and J. Nagaraju, Surface Electrode Switching of A 16-Electrode Wireless EIT System Using RF-Based Digital Data Transmission Scheme With 8 Channel Encoder/Decoder ICs, Measurement 45 (2012) 541–555.
- [9] W. A. Kalender, Computed Tomography: Fundamentals, System Technology, Image Quality, Applications, Publicis; 3 Ed. (2011).

- [10] G. Andria, F. Attivissimo, A. M. L Lanzolla, A statistical approach for MR and CT images comparison, Measurement 46 (2013) 57-65.
- [11] T. J. Yorkey and J. G. Webster, A comparison of impedance tomographic reconstruction algorithms, Clin. Phys. Physiol. Meas., 1987, Vol. 8, Suppl. A, 55-62.
- [12] T. K. Bera, S. K. Biswas, K. Rajan and J. Nagaraju, Improving Image Quality in Electrical Impedance Tomography (EIT) Using Projection Error Propagation-Based Regularization (PEPR) Technique: A Simulation Study, Journal of Electrical Bioimpedance, vol. 2, pp. 2–12, 2011.
- [13] T. K. Bera S. K. Biswas, K. Rajan and J. Nagaraju, Improving Conductivity Image Quality Using Block Matrix-based Multiple Regularization (BMMR) Technique in EIT: A Simulation Study, Journal of Electrical Bioimpedance, vol. 2, pp. 33–47, 2011.
- [14] T. K. Bera, S. K. Biswas, K. Rajan and J. Nagaraju, Image Reconstruction in Electrical Impedance Tomography (EIT) with Projection Error Propagation-based Regularization (PEPR): A Practical Phantom Study, Lecture Notes in Computer Science, Springer, 2012, Volume 7135/2012, 95-105, ADCONS 2011.
- [15] T. K. Bera, S. K. Biswas, K. Rajan and J. Nagaraju, Improving the Image Reconstruction in Electrical Impedance Tomography (EIT) with Block Matrix-based Multiple Regularization (BMMR): A Practical Phantom Study, IEEE World Congress on Information and Communication Technologies 2011(WICT-2011), India, University of Mumbai, Mumbai, India, 2011, pp 1346-1351.
- [16] D. S. Holder, Clinical and Physiological Applications of Electrical Impedance Tomography, Taylor & Francis; 1 edition (July 1, 1993)
- [17] R. H. Bayford, Bioimpedance Tomography (Electrical Impedance Tomography), Annual Review of Biomedical Engineering, Vol. 8: 63-91 (Volume publication date August 2006).
- [18] J. G. Webster, Medical Instrumentation Application and Design, Wiley; 4 edition (February 3, 2009).
- [19] M. Z. U. Rahmana, G.V.S. Karthik, S.Y. Fathima, A. Lay-Ekuakille, An efficient cardiac signal enhancement using time– frequency realization of leaky adaptive noise cancelers for remote health monitoring systems, Measurement 46 (2013) 3815–3835.
- [20] R. Khandpur, Biomedical Instrumentation: Technology and Applications, McGraw-Hill Professional; 1 edition (2004)
- [21] T. K. Bera and J. Nagaraju, A Multifrequency Constant Current Source for Medical Electrical Impedance Tomography, Proceedings of the IEEE International Conference on Systems in Medicine and Biology 2010 (IEEE ICSMB 2010), India, 16th-18th Dec'2010, Kharagpur, India, pp 278-283.
- [22] K. G. Boone, D. S. Holder, Current approaches to analogue instrumentation design in electrical impedance tomography, Physiol Meas. 1996 Nov;17(4):229-47.
- [23] T. K. Bera and J. Nagaraju, A Study of Practical Biological Phantoms with Simple Instrumentation for Electrical Impedance Tomography (EIT), Proceedings of IEEE International Instrumentation and Measurement Technology Conference (I2MTC2009), Singapore, 5th - 7th May 2009, pp 511-516.
- [24] T. I. Oh, H. Wi, Y do Kim, P. J. Yoo, E.J. Woo, A fully parallel multi-frequency EIT system with flexible electrode configuration: KHU Mark2, Physiol Meas. 2011 Jul;32(7):835-49.
- [25] Li JH, Joppek C, Faust U., Fast EIT data acquisition system with active electrodes and its application to cardiac imaging, Physiol Meas. 1996 Nov;17 Suppl 4A:A25-32.
- [26] P. J. Riu, J. Rosell, A. Lozano, R. Pallà-Areny, Multi-frequency static imaging in electrical impedance tomography: Part 1 instrumentation requirements, Medical and Biological Engineering and Computing, November 1995, Volume 33, Issue 6, pp 784-792.
- [27] T. K. Bera and J. Nagaraju, Sensors for Electrical Impedance Tomography, The Measurement, Instrumentation, and Sensors Handbook, 2nd Edition, Ed: John G. Webster, CRC Press, 2013.
- [28] Jossinet J, Tourtel C, Jarry R., Active current electrodes for in vivo electrical impedance tomography, Physiol Meas. 1994 May;15 Suppl 2a:A83-90.
- [29] Rahal M, Khor JM, Demosthenous A, Tizzard A, Bayford R., A comparison study of electrodes for neonate electrical impedance tomography, Physiol Meas. 2009 Jun;30(6):S73-84.

- [30] Koukourlis CS, Kyriacou GA, Sahalos JN., A 32-electrode data collection system for electrical impedance tomography, IEEE Trans Biomed Eng. 1995 Jun;42(6):632-6.
- [31] T. K. Bera and J. Nagaraju, Studying the Resistivity Imaging of Chicken Tissue Phantoms with Different Current Patterns in Electrical Impedance Tomography (EIT), Measurement, 45 (2012) 663–682.
- [32] T. K. Bera and J. Nagaraju, A Stainless Steel Electrode Phantom to Study the Forward Problem of Electrical Impedance Tomography (EIT), Sensors & Transducers Journal, Vol. 104, Issue 5, May 2009, pp. 33-40.
- [33] T. K. Bera and J. Nagaraju, A Multifrequency Electrical Impedance Tomography (EIT) System for Biomedical Imaging, IEEE International Conference on Signal Processing and Communications (SPCOM 2012), Bangalore, India pp 1-5.
- [34] T. K. Bera and J. Nagaraju, A Gold Sensors Array for Imaging The Real Tissue Phantom in Electrical Impedance Tomography, International Conference on Materials Science and Technology 2012 (ICMST 2012), Kottayam, Kerala, India.
- [35] T. K. Bera and J. Nagaraju, Electrical Impedance Spectroscopic Study of Broiler Chicken Tissues Suitable for The Development of Practical Phantoms in Multifrequency EIT, Journal of Electrical Bioimpedance, vol. 2, pp. 48–63, 2011.
- [36] Schneider ID, Kleffel R, Jennings D, Courtenay AJ., Design of an electrical impedance tomography phantom using active elements, Med Biol Eng Comput. 2000 Jul;38(4):390-4.
- [37] Sperandio M, Guermandi M, Guerrieri R., A four-shell diffusion phantom of the head for electrical impedance tomography, IEEE Trans Biomed Eng. 2012 Feb;59(2):383-9.
- [38] T. K. Bera and J. Nagaraju, A Chicken Tissue Phantom for Studying An Electrical Impedance Tomography (EIT) System Suitable for Clinical Imaging, Sensing and Imaging: An International Journal, Volume 12, Numbers 3-4, 95-116, 2011.
- [39] Griffiths H., A phantom for electrical impedance tomography, Clin Phys Physiol Meas. 1988;9 Suppl A:15-20.
- [40] D. Isaacson, J. Mueller, J.C. Newell, S. Siltanen, Reconstructions of Chest Phantoms by the D-Bar Method for Electrical Impedance Tomography, Trans. Med. Imag., Vol. 23, No. 7, 2004
- [41] P. Druilheta, A. Momb, PLS regression: A directional signal-tonoise ratio approach, Journal of Multivariate Analysis, Volume 97, Issue 6, July 2006, Pages 1313–1329
- [42] Tidswell AT, Bagshaw AP, Holder DS, Yerworth RJ, Eadie L, Murray S, Morgan L, Bayford RH., A comparison of headnet electrode arrays for electrical impedance tomography of the human head, Physiol Meas. 2003 May;24(2):527-44.
- [43] S. Sumathi, P. Surekha, LabVIEW based Advanced Instrumentation Systems, Springer, 1 edition (April 19, 2007)
- [44] Z. Wang, Y. Shang, J. Liu, X. Wu, A LabVIEW based automatic test system for sieving chips, Measurement, 2013, 46(1), 402-410.
- [45] F. C. Alegria, E. Martinho, F. Almeidac, Measuring soil contamination with the time domain induced polarization method using LabVIEW, Measurement 42 (2009) 1082–1091
- [46] T. K. Bera, Manobjyoti Saikia, J. Nagaraju, A Battery-based Constant Current Source (Bb-CCS) for Biomedical Applications, 2013 International Conference on Computing, Communication and Networking Technologies (ICCCNT 2013), July 4-6, 2013, India.
- [47] N. Polydorides and W.R.B. Lionheart, AMatlab toolkit for threedimensional electrical impedance tomography: a contribution to the Electrical Impedance and Diffuse Optical Reconstruction Software project, Meas. Sci. Technol. 13 (2002) 1871–1883
- [48] T. K. Bera and J. Nagaraju, Studies and Evaluation of EIT Image Reconstruction in EIDORS with Simulated Boundary Data, International conference on soft computing for problem solving (SocProS 2012), Dec. 28-30, 2012, Jaipur, India.
- [49] M. Vauhkonen, W. R. Lionheart, Heikkinen LM, Vauhkonen PJ, Kaipio JP., A MATLAB package for the EIDORS project to reconstruct two-dimensional EIT images, Physiol Meas. 2001 Feb; 22(1):107-11.